

UNITED STATES PATENT APPLICATION

of

Ian H. Campbell

and

Darryl L. Smith

for

**CHEMICAL AND BIOLOGICAL SENSOR USING
ORGANIC SELF-ASSEMBLED TRANSISTORS**

MADSON & METCALF, P.C.

ATTORNEYS AT LAW

900 GATEWAY TOWER WEST

15 WEST SOUTH TEMPLE

SALT LAKE CITY, UTAH 84101-4000

BACKGROUND OF THE INVENTION

Government Rights

This invention was made with Government support under Contract Number W-7405-ENG-36 awarded by the United States Department of Energy to the Regents of the University of California. The Government has certain rights in the invention.

Field of the Invention

The present invention relates generally to organic semiconductor transistors. More specifically, the present invention applies to organic self-assembled transistors for use with chemical and biological sensor applications.

Description of Related Art

Air quality has long been an important health concern. For example, miners used to bring a canary or other small sensor bird down into the mine to warn them if the air quality changed. If the air became dangerous the little sensor bird would stop chirping and in a worst-case die, thereby warning the miners to clear out of the area. Unfortunately, this type of "live" biological sensor exhibited many of the same problems that face modern biological and chemical sensors. Namely, it was very difficult to obtain immediate quantitative and qualitative information from the sensor. If the bird died, there was no way to determine exactly what type of vapor killed it (qualitative) or whether the death was a result of prolonged low-level exposure or of brief exposure to a saturated wave of poisonous gas (quantitative). Presently, modern resistor based sensors continue to have difficulty distinguishing related vapor molecules from each other, such as ethanol from methanol. In addition, residual amounts of vapor left on the sensor

1 following exposure to ambient, reduce the sensor accuracy and require sensor
2 recalibration. In addition, unless someone was assigned to watch the sensor bird, there
3 was still a risk that the sensor bird would die without being noticed. Also, it was
4 necessary for the person monitoring the sensor bird to be in the vicinity of the sensor to
5 properly read it, exposing himself or herself to unnecessary risk. Most modern sensors,
6 like the bird, require a large quantity or threshold of vapor be present before the sensor
7 can give a warning response. With extremely toxic substances this warning may be too
8 late to prevent dangerous exposure.

9 Many of these same biological sensor characteristics continue to plague modern
10 chemical and biological sensors. For example, the detection accuracy of modern sensors
11 deteriorates over time. This deterioration requires that the filters be replaced in order to
12 maintain the accuracy of the sensor. This sensitivity deterioration also makes calibration
13 a difficult process. The more comprehensive that the sensor is in detecting various
14 analyte molecules, the more complex the calibration process for that sensor becomes.
15 Also, each supplemental class of molecules detected by a sensor often requires additional
16 electronics. As such the available comprehensive environmental sensors are often too
17 large to be considered portable. Attempts to reduce sensor component size via inorganic
18 and organic transistors have met with difficulty.

19 Specifically, electronic devices based on doped organic materials have not been
20 developed as completely as doped inorganic semiconductors making response modeling
21 of organic transistors unpredictable. Further, obtaining robust n-type and p-type doping
22 of organic materials suitable for electronic device development has also proven difficult.
23 Doped conducting materials, such as acid doped polymers, have electrical properties
24

1 similar to low conductivity metals. Presently inorganic thin-film transistors employ
2 undoped semiconductor layers and doped semiconductor contacts.

3 In contrast, conventional doped, inorganic transistors operate in either a charge
4 accumulation or charge inversion mode, neither mode satisfying the previously
5 mentioned sensor requirements. For example, a p-channel transistor in a charge inversion
6 regime uses p-type semiconductor contacts and an n-type doped semiconductor layer in
7 which the channel is formed. When sufficient gate bias is applied to the structure, an
8 inversion layer is formed consisting of a thin p-type region in the n-type doped
9 semiconductor adjacent to the gate insulator (the channel). The p-type doped
10 semiconductor contacts make good electrical contact only to this inversion layer. In the
11 "off" state, the leakage current is very low because the structure consists of a reverse
12 biased diode in series with a forward biased diode. This high "off" state resistance is one
13 advantage of doped inorganic transistors. Unfortunately, inorganic transistors are not as
14 receptive to adsorption of vapor molecules and are thus less accurate.

15 Transistors operating in the accumulation regime utilize doped organic or
16 semiconductor layers but, instead of forming an inversion layer, the channel is formed by
17 biasing the gate to accumulate charge of the same type as the layer doping. For example,
18 a p-type transistor has the gate biased so that additional holes accumulate adjacent to the
19 gate insulator. Devices operating in the accumulation regime have large leakage currents
20 and their total current is sensitive to the organic layer thickness. The poor leakage
21 current and sensitivity to film thickness occur because the contacts are not rectifying, as
22 they are in the inversion regime, so current can flow through the doped regions of the
23 organic material independent of the gate bias. Therefore, it is not desirable to operate in
24 an accumulation regime.

1 Additionally, the charge transport properties of organic materials, particularly at
2 high carrier densities, are not very well understood. There are substantial discrepancies
3 between a conventional inorganic FET model and organic device measurements. The
4 most important properties to be included in an organic model are the charge density, the
5 electric field dependence of the carrier mobility, and the contact interface electronic
6 structure. These properties are important because the charge density and electric field in
7 the organic material vary by many orders of magnitude. Including an accurate
8 description of the mobility is important for calculating the charge density and potential
9 profiles within the organic device. Modern organic models are analyzed using inorganic
10 thin film transistor models, which use independent mobility, electric field, and charge
11 density while ignoring the details of the interaction surrounding the contacts.

MADSON & METCALF, P.C.
ATTORNEYS AT LAW
900 GATEWAY TOWER WEST
SUITE 1500
SAN FRANCISCO, CALIFORNIA 94111
(415) 774-2200
FAX (415) 774-2201
WWW.MADSONMETCALF.COM

SUMMARY OF THE INVENTION

The present invention provides an array of specialized sensor transistors easily tailored for sensor array or electronic nose applications. These qualities are primarily accomplished through an organic self-assembled monolayer exposed to the atmosphere. The monolayer is used in the sensor transistor as the active semiconductor layer in which the conducting channel is formed. Each transistor may be customized to detect molecules adsorbed on the organic self-assembled monolayer. The chemical specificity and strength of interaction of the monolayer may be selectively tuned by varying the chemical or sensing end group of the organic molecules comprising the monolayer. The adsorbed molecules are identified using the voltage characteristics, such as mobility and density of charge carriers, of the sensor transistors, which are very sensitive to vapor molecules. The sensor transistor can also be easily cleaned and recalibrated by heating the monolayer to repel the adsorbed molecules from the detection surface. The sensor transistor used in the present invention may be constructed using known low-cost Very Large Scale Integration (VLSI) silicon fabrication processes with the added step of micro-printing the sensitive organic self-assembled monolayer onto the sensor transistor after the high temperature processing.

The present invention has been developed in response to the current state of the art, and in particular, in response to these and other problems and needs that have not been fully or completely solved by currently available sensor or electronic nose applications. Thus, it is an overall object of the present invention to provide chemical and biological sensors via organic self-assembled transistors. This can be accomplished by operating the organic transistor with an organic self-assembled monolayer in a charge injection mode. An example of a sensor transistor using an organic self-assembled

1 monolayer is shown in Figures 1-3. Figures 4 and 5 illustrate the responses of one
2 embodiment of the present invention using fabricated organic transistors with a thin
3 organic film, such as pentacene, as the active semiconductor layer.

4 Accordingly, one advantage the sensor transistor provides, while maintaining a
5 desired diminutive overall size and cost, is an atomically sensitive surface that may be
6 easily customized for various detection purposes. Other solutions, which may be
7 available, compromise one of these elements.

8 Another advantage of the sensor transistor is that it may distinguish related vapor
9 molecules from each other using transistor response, such as differential response.

10 Yet another aspect of the sensor transistor is the low threshold of vapor required
11 before the sensor gives a warning response.

12 Another advantage of the sensor transistor is that the detection accuracy and
13 calibration is easily maintained by periodic cleansing via relatively high current pulses
14 that heat the organic layer and drive off adsorbed molecular species.

15 Additional objects and advantages of the invention will be set forth in the
16 description which follows, and in part will be obvious from the description, or may be
17 learned by the practice of the invention. The objects and advantages of the invention may
18 be realized and obtained by means of the instruments and combinations particularly
19 pointed out in the appended claims. These and other objects and features of the present
20 invention will become more fully apparent from the following description and appended
21 claims, or may be learned by the practice of the invention as set forth hereinafter.

MADSON & METCALF, P.C.
ATTORNEYS AT LAW
900 GATEWAY TOWER WEST
WEST SOUTHTHEMPL
SHEET LAKE CITY, UT 84103

Figure 7 is a block diagram illustrating an exemplary sensor system that provides a suitable operating environment for one embodiment of the present invention.

1 **DETAILED DESCRIPTION OF THE PREFERRED EMBODIMENTS**

2 Figure 1 and the following discussion are intended to provide a brief, general
3 description of a suitable operating environment in which the invention may be
4 implemented. Figure 1 is intended to be illustrative of potential systems that may utilize
5 the present invention and is not to be construed as limiting. Those skilled in the art will
6 appreciate that the invention may be practiced with many types of configurations,
7 including organic transistors, self-assembled, and the like.

8 Reference is first made to Figure 1, an organic transistor 100 or environment in
9 which the present invention may be utilized or implemented. Organic transistors 100 are
10 lateral devices consisting of a source electrode 104, drain electrode 106, a gate insulator
11 108, and a conducting gate contact 110. When a bias is applied between the gate 110 and
12 source/drain electrodes 104 and 106, charges are injected into the organic film 102 from
13 the source 104 and drain 106 contacts. With an additional bias applied between the
14 source 104 and drain 106 contacts, a current flows laterally between these two contacts.
15 The source to drain current is modulated by the gate voltage producing the transistor
16 action.

17 Typically the organic transistors use undoped, insulating organic materials as the
18 charge-transporting layers. The charge carriers in the devices are injected from the
19 contacts. Because the organic material in which the channel is formed is undoped, all of
20 the charge in the channel is injected from the contacts. At zero gate bias, the organic
21 material contains no free charges except for a thin region (a few nanometers) near the
22 contacts that contain charge thermally excited from the metals into the organic material.
23 When a gate bias is applied to the structure, charges are injected into the organic material
24 from both the source and drain contacts, forming a thin sheet of charge adjacent to the

1 gate insulator (the channel). In the "on" state, the current flows through this thin sheet of
2 charge. In the "off" state, the leakage current is low because of the high intrinsic
3 resistivity of the undoped organic film. The substrate comprises a semiconductive
4 material, such as silicon substrate 112.

5 The contacts are preferably Space Charge Limited (SCL) contacts, but those of
6 skill in the art know that other contacts may also be used. SCL contacts provide the
7 maximum current that the organic semiconductor material can support. These SCL
8 contacts have a small energy barrier, less than about 0.3 eV, between the metal Fermi
9 energy and the conduction or valence levels of the organic semiconductor. The small
10 energy barrier allows SCL contacts to provide the maximum current. In contrast, non-
11 SCL or Schottky contacts have a relatively large energy barrier, greater than about 0.4
12 eV, between the metal Fermi energy and the conduction or valence levels of the organic
13 semiconductor. The large energy barrier blocks current flow from the metal to the
14 semiconductor. Organic transistors that use non-SCL contacts thus require larger
15 voltages and thus more power to achieve the same current and chemical sensitivity as
16 transistors using SCL contacts.

17 The recent development of low operating voltage (about 5V) organic
18 semiconductor transistors combined with progress in organic self-assembly techniques
19 presents an opportunity to create a new class of organic self-assembled transistors
20 (OSAT) 100 ideal for chemical and biological sensor applications. The OSAT 100 uses
21 an organic self-assembled monolayer 102 as the active, semiconductor layer in which the
22 conducting channel of the OSAT 100 is formed. The current is carried in this organic
23 monolayer 102, about 3 nm thick, which is directly exposed to ambient. Since the current
24 is carried in this surface monolayer 102, the current-voltage characteristics of the

1 transistor are very sensitive to vapor molecules 114. The vapor molecules 114 change
2 both the mobility and density of the charge carriers in the organic film 102. Each
3 molecule produces distinct changes in the OSAT 100 response that can be used to
4 identify the vapor molecule 114.

5 The OSAT 100 is fully compatible with silicon very large scale integration
6 (VLSI) technology since the active organic monolayer 102 can be added after all of the
7 high temperature silicon processing is completed. A schematic of an OSAT 100
8 fabricated on a silicon substrate 112 is shown in Figure 1. In one embodiment of the
9 invention, the semiconductor layer is the organic self-assembled monolayer 102, the
10 source 104 and drain 106 contacts are metals, such as Al or Au, the gate insulator 108 is a
11 high dielectric constant oxide, such as Ytria Stabilized Zirconia (YSZ), and the gate
12 contact 110 is n+ silicon. The insulator 108 has a dielectric constant greater than about 4.
13 The organic self-assembled monolayer 102 is deposited after the insulator 108 and
14 contact layers 104 and 106 are fabricated so that the transistor can be made on a silicon
15 VLSI substrate 112. The organic monolayer 102 can be extremely thin (< 10 nm)
16 because the charge in the organic layer forming the channel is electrostatically confined
17 to the organic material only a few nm from the gate insulator 108. The transport
18 properties of the thin organic layer are very sensitive to adsorbents on the surface of the
19 monolayer 102. This sensitivity to adsorbents on the thin organic layer is the basis for
20 the sensitivity of OSAT 100 based chemical and biological sensors.

21 The active layer of the OSAT 100 is a conjugated organic monolayer 102 that is
22 directly exposed to the atmosphere to be probed. The self-assembly chemistry used to
23 form the monolayer produces dense, defect free layers that are covalently bonded to the
24 substrate and to each other. The monolayer is very stable physically and chemically.

1 The length and surface density of the molecules in a typical conjugated organic
2 monolayer 102 is about 3 nm long and covers about 10^{-14} cm². One embodiment of
3 transistor structure with a monolayer area of 10^{-6} cm² (100 μ m wide by 1 μ m gate length)
4 has a monolayer volume of 3×10^{-13} cm³ and contains 10^8 organic molecules. Because
5 the molecular layer is only a few nm thick, molecules adsorbed on its surface can have a
6 strong effect on its properties. To detect small organic molecules, the transistor sensor
7 could have a maximum response (assuming 1 molecule to be sensed on the surface of
8 each molecule comprising the monolayer) with only 10^8 adsorbed molecules or about
9 10^{-16} moles. It is possible to measure the transistor response well below the maximum
10 surface coverage. This very small number of analyte molecules required for maximum
11 response implies that the sensor can detect very low concentrations of volatile
12 compounds and respond very quickly to moderate vapor concentrations.

13 Organic self-assembled transistors can be made by assembling the organic
14 monolayer 102 on the gate insulator 108 of transistor structures produced on silicon VLSI
15 substrates 112. The VLSI substrate 112 would contain the gate insulator 108, gate 110,
16 source contact 104, and drain contact 106 of the OSAT in addition to conventional silicon
17 circuitry for readout and processing. An appealing method to deposit a wide range of
18 organic monolayers 102 is to use micro-contact printing (MCP), a low cost fabrication
19 process. In MCP, an elastomeric stamp is used to transfer the monolayer 102 to the
20 substrate 112 and insulator 108 by physical contact. The stamp is shaped so that when it
21 is pressed against the insulator 108 or substrate 112, the monolayer molecules 200 are
22 transferred from the stamp to the substrate 112 in the desired pattern. This technique has
23 been demonstrated to have submicron spatial resolution. The quality of the self-

1 assembled monolayers 102 formed using this procedure is as good or better than layers
2 formed using solution methods.

3 To produce a large array of sensors with different monolayers, the substrate
4 would be printed multiple times using stamps with different patterns inked with different
5 molecules for each distinct monolayer. Another feature of using robust silicon structures
6 is that the silicon circuitry and substrate can be reused. To reuse the structures only the
7 organic monolayers need to be removed, in fact only a portion of the monolayer need be
8 replaced for recalibration to occur. Complete removal could be accomplished using a
9 short plasma etch with oxygen or hydrogen if the silicon circuitry is properly
10 encapsulated. A new monolayer could then be applied to the substrate to form a new
11 OSAT.

12 Figure 2A is a schematic view of the molecules used to form the organic self-
13 assembly monolayer shown in Figure 1. The self-assembly molecule 200 consists of a
14 conjugated segment 204 with two end groups, a sensing end group 202, and an attaching
15 end group 206.

16 The organic molecules used to form the self-assembled monolayer 102 consist of
17 a conjugated segment 204 that carries the transistor current terminated by two functional
18 end groups. One attaching end group 206 is used to covalently attach the molecule to the
19 gate insulator 108 (and to neighboring molecules in the self-assembled monolayer) and
20 the other sensing end group 202 defines the chemistry of the surface used to sense vapor
21 molecules. As illustrated in Figure 2B, one can use the same attaching end group 206 to
22 attach to the insulator 108 and the same conjugated molecule 204 to carry the current
23 varying only the terminal sensing end group 202 that determines the sensor interaction. It
24 is therefore possible to produce an array of transistor sensors with very similar initial I-V

1 characteristics (same current carrying molecule) but that interact very differently with the
2 atmosphere due to variations in the sensing end group 202.

3 This property makes it convenient to make large arrays by combining multiple
4 sensor elements. Each sensor element uses identical electronics for common sensor
5 functions, such as the readout components, but allow for an almost unlimited range of
6 detection responses on the sensor transistors via variations to the sensing end group 202.
7 Exemplary sensing end groups 202 include halides, nitriles, ketones, amines, amides and
8 the like. Halides are useful for detecting alcohols, amides, and acids. While sensing end
9 groups 202 that use nitrile help detect NO_x, amino acids, and proteins. Ketone may be
10 used as a sensing group for detecting esters. The amines and amides are useful in
11 detecting halides and bases.

12 Exemplary conjugated segments 204 include Phenyl-acetylene and Phenylene-
13 vinylene. Figure 2B illustrates the molecular structure of a conjugated segment 204 using
14 Phenyl-acetylene. Phenyl-acetylene segments 204 exhibit several useful properties, for
15 example they are very rigid and form high areal density monolayer films. The rigidity
16 and high packing density allow charges to move efficiently through conjugated segments
17 204 comprising Phenyl-acetylene. An alternative embodiment uses phenylene-vinylene
18 conjugated segments 204, which are useful for sensing small molecules, such as methane,
19 silane, methanol, and the like.

20 Figure 2B further illustrates the molecular structure of a trichlorosilyl group used
21 as an attaching end group 206. The trichlorosilyl group is one preferred family of
22 attaching end groups 206, because they produce the strongest and most durable organic
23 semiconductor layer. These trichlorosilyl based attaching end groups 206 form strong
24 covalent bonds to the oxide surface and to each other. Other exemplary attaching end

1 groups 206 include amine and carboxylic acid groups. These groups form relatively
2 weak ionic bonds to the oxide surface, which may be suitable for disposable or field
3 produced/repairable sensors.

4 Figure 3 illustrates the ambient state of a self-assembled monolayer channel for
5 use with the present invention as illustrated in Figure 1. Specifically, the sensing end
6 group surface 302 is in contact with ambient conditions. A close up schematic of the
7 OSAT 300 is also shown in Figure 3. The use of self-assembly techniques allows the
8 fabrication of a dense, highly ordered organic monolayer 102 with an atomically sharp
9 interface in the sensing end group surface 302. Changing the sensing end group 202 of
10 the molecule can control the chemical properties of the sensing surface 302. The
11 conjugated segment 204 and attaching end group 206 can be kept constant. It is therefore
12 possible to produce an array of transistor sensors with very similar initial I-V
13 characteristics (same current carrying molecules) but that interact very differently with
14 the atmosphere due to variations in the sensing end group 202. This property makes it
15 convenient to make large arrays using identical electronic readout components and still
16 allow a wide range of responses. The ability to combine a very large number of sensor
17 interactions on a convenient silicon VLSI template allows production of chemical and
18 biological sensors that can detect and distinguish a large number of volatile compounds.

19 Analogous to inorganic transistors, organic self-assembled transistors can be n-
20 channel or p-channel devices. For OSAT sensor applications, this can be significant
21 since the positive or negatively charged channel is only a few angstroms from the
22 molecule to be detected. The proximity of the charged channel and the vapor molecule
23 means that electrostatic interactions could be used to distinguish molecules. For
24 example, a molecule with a permanent dipole moment would orient itself differently on

1 the surface of opposite polarity devices. The change in orientation would produce a
2 different effect on the transistor characteristics. Unlike conventional inorganic
3 transistors, the polarity of the organic transistor is largely determined by the type of metal
4 used for the drain and source contacts. The organic material is undoped and the charge is
5 injected into the molecule directly from the contacts. One embodiment of n-channel
6 devices uses low work function metals (e.g. Al). While another embodiment of p-
7 channel devices uses high work function metals (e.g. Au). Thus, it is possible to produce
8 arrays of n- and p-channel devices using the same organic molecules within a sensor
9 device simply by using different metal contacts on the silicon substrate.

10 Restoring the transistor 300 following a detection cycle requires removal of
11 adsorbed molecules from the sensing end group surface 302 so that the transistor 300 can
12 respond to its ambient with a clean surface. Because the drain-source resistance can be
13 varied over many orders of magnitude, it is possible, using conventional circuitry, to use
14 relatively high current pulses to heat the organic layer and drive off adsorbed molecular
15 species. Very little energy is required to heat the thin organic film. Assuming an organic
16 monolayer volume of $3 \times 10^{-13} \text{ cm}^3$ (see above) the energy required to heat the layer 50°C
17 is only 15 pJ. For example, the low current transistor response can be measured
18 frequently and when a significant response is detected the surface could be thermally
19 cleaned to refresh or reset the transistor sensor. This enables increased sensitivity and
20 more rapid response times by cleaning the interacting surface of adsorbed molecules.

21 As previously described, organic self-assembled transistors used for chemical and
22 biological sensor applications provide several advantages over the existing art, such as:
23 1) monolayer sensitivity, 2) chemically tailored surface, 3) spectroscopic readout, 4)
24

1 silicon VLSI compatibility, 5) complementary polarity devices, and 6) thermal surface
2 cleaning.

3 To illustrate the advantages of spectroscopic readout of organic self-assembled
4 transistors for chemical and biological sensor applications, Figures 4 and 5 show
5 responses of fabricated organic transistors using thin organic films as the active
6 semiconductor layer. The transistors were fabricated on silicon substrates using Pt source
7 and drain contacts and YSZ as the gate insulator. Pentacene films about 10 nm thick
8 were used in place of the organic self-assembled monolayer. The transistor current-
9 voltage characteristics at fixed gate voltage are shown in Figure 4. A transistor is a three
10 terminal device and thus its current-voltage (I-V) characteristics contain more
11 information than those of two terminal devices such as resistors. The I-V characteristics
12 are often presented as shown in Figure 4 where the drain-source current is shown as a
13 function of drain-source voltage at a fixed gate bias.

14 The transistor characteristics are usually described by its gate threshold voltage
15 and charge carrier mobility. The transistor response to a molecule 114 on its surface 302
16 will affect both of these parameters. The control of sensing end group surface properties
17 302 based on varying the end groups of organic self-assembled monolayers is well
18 known to one of skill in the art. For example, the transistor responses from a variety of
19 surfaces 302 with different adsorption isotherms, electron withdrawing, or electron
20 donating groups can be used to identify vapor species. Therefore, it is possible to
21 distinguish vapor molecules absorbed on the surface 302 based on the transistor response
22 as a function of drain-source and/or gate-source voltage. Measuring this rich set of data
23 from transistor sensors will facilitate discriminating and identifying target compounds.
24

1 The I-V characteristics shown in Figure 4 are for the following exposure
2 conditions: ambient 401, and 1 part-per-thousand each of ethanol 402, methanol 404, o-
3 xylene 406, p-xylene 408, and tetrahydrofuran (THF) 410. In all cases, exposure to the
4 vapor decreases the drain-source current 412. The changes in the drain-source current
5 412 are functions of the drain-source voltage 414, that is, the shape of the I-V curves are
6 different for each molecule. The change in shape of the I-V characteristic shows that it is
7 possible to distinguish molecules from their distinct responses as a function of voltage.

8 To illustrate this, consider the differential response 512, R, of the transistor as
9 illustrated in Figure 5. The differential response 512 is the derivative of the drain-source
10 current with respect to the drain-source voltage of the reference ambient response divided
11 by the derivative of the drain-source current with respect to the drain-source voltage of
12 the sensor gas response at constant gate voltage, as illustrated by equation 1:

$$R = \frac{\left(\frac{\partial I_R}{\partial V_R} \right)}{\left(\frac{\partial I_S}{\partial V_S} \right)_{V_G}}$$

Equation 1

17 Where I_R is the drain-source current and V_R is the drain-source voltage of the reference
18 ambient response. While I_S is the drain-source current and V_S is the drain-source voltage
19 of the sensor gas response.

20 Figure 5 illustrates the differential response 512 of the transistor upon exposure to
21 different vapors. The alcohol 502 and 504, xylene 506 and 508, and THF 510 molecules
22 have substantially different differential responses as a function of voltage. The two
23 alcohol molecules 502 and 504 have peaks about 5-6V and the two xylene molecules 506
24

1 and 508 have peaks about 2-3V. The THF molecule 510 has a sharper peak about 3V.
2 Furthermore, ethanol 502 can be distinguished from methanol 504 and o-xylene 506
3 distinguished from p-xylene 508 using this analysis. The large amount of information
4 available from a single organic transistor in a chemical/biological sensor array adds
5 significantly to its ability to discriminate and identify molecules. The response time of
6 these organic thin-film transistors is a few seconds at concentrations of about one part per
7 thousand. The response time of organic self-assembled transistors is even faster. The
8 response time of the organic thin-film transistors is limited by the time required for the
9 gas molecules to diffuse through part of the thin organic film to reach the conducting
10 channel. The OSATs do not have this delay.

11 Figure 6 illustrates an exemplary sensor 600 in accordance with one embodiment
12 of the present invention. The organic monolayer fabrication capabilities previously
13 discussed, such as MCP, help produce a novel class of extremely versatile and sensitive
14 chemical and biological sensors 600. Specifically, the exemplary sensor 600 includes an
15 array 610 of organic self-assembled transistors 100 that may be individually monitored
16 by a processing module 620 using conventional circuitry 630, such as a data bus.

17 The array 610 may be constructed using known low-cost VLSI silicon fabrication
18 processes with the added step of micro-printing a customized sensitive organic self-
19 assembled monolayer onto each sensor transistor 100. Using an organic self-assembled
20 monolayer as the active semiconductor layer in which the conducting channel is formed
21 in transistors 100, the present invention is able to provide an array 610 of specialized
22 transistors 100 easily tailored for sensor array or electronic nose applications. Each
23 transistor 100 is customized to detect molecules adsorbed on the organic self-assembled
24 monolayer exposed to the atmosphere. The adsorbed molecules are identified using the

1 voltage characteristics, such as mobility and density of charge carriers, of the sensor
2 transistors 100, which are very sensitive to vapor molecules. The chemical specificity
3 and strength of interaction of the monolayer may be selectively tuned by varying the
4 chemical or sensing end group of the organic molecules comprising the monolayer. The
5 array 610 can also be easily cleaned and recalibrated by heating the monolayer of each
6 transistor 100 to repel the adsorbed molecules from the detection surfaces.

7 In various embodiments, the processing module 620 controls the operation of the
8 array 610, including the other components thereof that are also connected to the
9 processing module 620. In addition to control functions, the processing module 620 also
10 receives and correlates detection data from the array 610 via conventional circuitry 630.
11 The detection data sent to the processing module 620 may include differential response
12 and voltage characteristics of the sensor transistors 100, such as the mobility and density
13 of charge carriers. In one embodiment, the processing module 620 compares the
14 detection data against expected characteristic transistor responses and indicates when
15 they do not match. The processing module may be embodied as a central processing unit
16 (CPU), a microcontroller, a microprocessor, a digital signal processor (DSP), a state
17 machine, a programmable logic device, an application specific integrated circuit (ASIC),
18 a general-purpose computing device, or other device known in the art.

19 Figure 7 and the following discussion are intended to provide a brief, general
20 description of a suitable environment in which the invention may be implemented.
21 Reference is first made to Figure 7 illustrating an exemplary sensor system 700 or
22 environment in which the present invention may be utilized or implemented. Figure 7 is
23 intended to be illustrative of potential systems that may utilize the present invention and
24 is not to be construed as limiting. Sensor system 700 uses a centrally located computer

1 710 in communication with various chemical and biological sensors 600 to monitor
2 sensor responses. This sensor configuration allows a detection perimeter to be monitored
3 from a central location. Another advantage of this remote sensor configuration is that
4 critical locations may be continual monitored without requiring the individual monitoring
5 the sensor to be in the proximity of the location.

6 Those skilled in the art will appreciate that the invention may be practiced with
7 many types of computer system configurations 710, including processing modules as
8 previously described, personal computers, hand-held devices, multi-processor systems,
9 microprocessor-based or programmable consumer electronics, network PCs,
10 minicomputers, mainframe computers, Personal Digital Assistants, and the like.

11 In one embodiment, the sensor 600 includes a plurality of organic self-assembled
12 transistors, in which each transistor is selectively tuned via sensing end groups to detect
13 different vapor molecules. In this manner the array of specialized transistors allow each
14 sensor 600 to remotely monitor multiple atmospheric conditions. One additional sensor
15 configuration analyzes transistor responses against expected threshold values prior to
16 transmitting detection data to the centrally located processing module 710. These sensors
17 600 partially incorporate the processing module locally, thereby reducing unnecessary
18 communication with a centralized sensor server.

19 The present invention may be embodied in other specific forms without departing
20 from its spirit or essential characteristics. The described embodiments are to be
21 considered in all respects only as illustrative and not restrictive. The scope of the
22 invention is, therefore, indicated by the appended claims rather than by the foregoing
23 description. All changes that come within the meaning and range of equivalency of the
24 claims are to be embraced within their scope.

What is claimed and desired to be secured by United States Letters Patent is:

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